

Controlled Release Theory

Last time:	tailoring the structure of degradable polymers Fundamental concepts in controlled release
Today:	Theory of degradable polymer-based controlled release
Reading:	Charlier et al., 'Release of mifepristone from biodegradable matrices: experimental and theoretical evaluations,' <i>Int. J. Pharm.</i> 200 , 115-120 (2000)

ANNOUNCEMENTS:

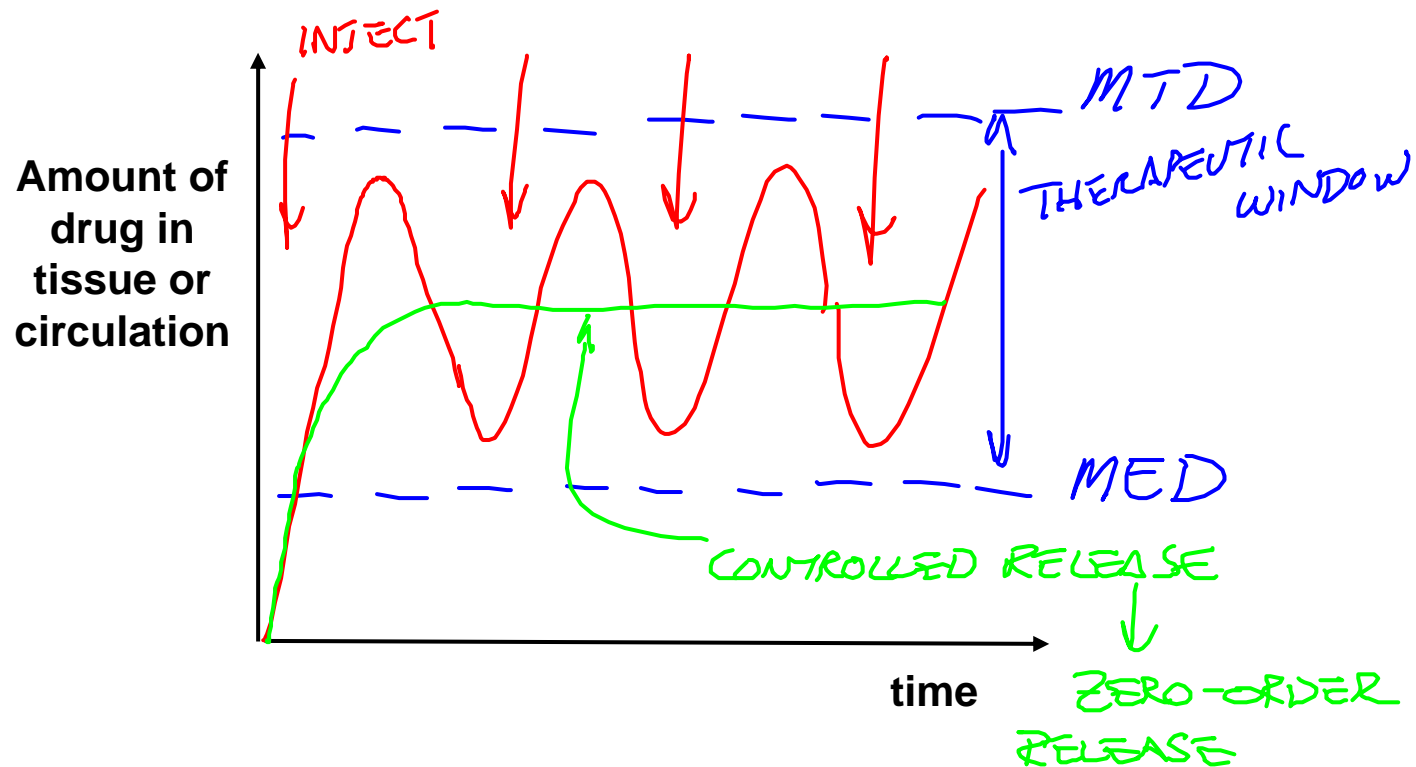
PS 1 DUE 5pm

PS 2 POSTED TOMORROW, DUE 1 WEEK LATER

Last time

Therapeutic index: tailoring materials to provide release kinetics matching the 'therapeutic window'

Bolus drug injection:

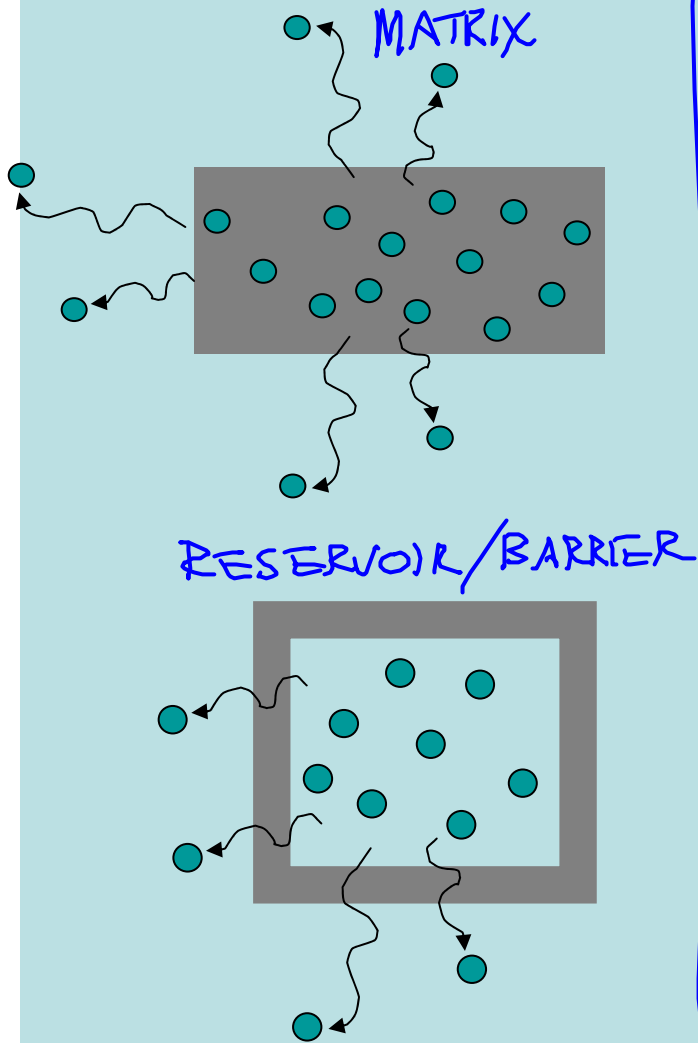


Mechanisms of controlled release

OVERVIEW OF MECHANISMS:

- DIFFUSION-BASED RELEASE
 - WATER INFUX-CONTROLLED RELEASE
- ERODING MATRIX
- REGULATED/TRIGGERED RELEASE

Drug diffusion-controlled release



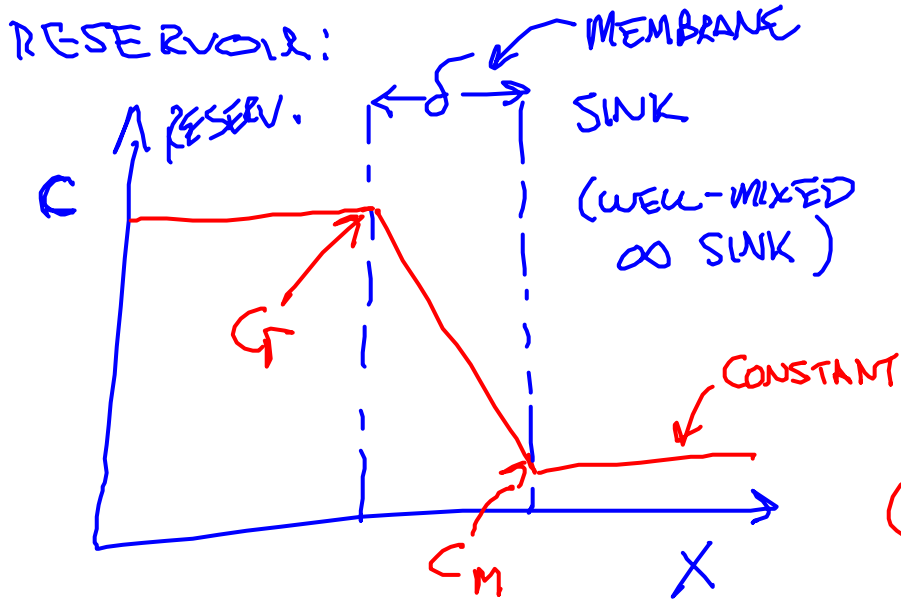
Advantage:

- WELL-DEFINED KINESIS
- ↓
- MODEL RIGOROUSLY

Disadvantages:

- NON-DEGRADABLE MATERIALS
- DIFFUSION OF MACROMOLECULES TOO SLOW TO BE USEFUL
- DANGER OF 'DOSE DUMPING' IN RESERVOIR SYSTEMS

Release kinetics for diffusion-controlled release



FICK'S FIRST LAW:

$$J = \text{FLUX} = \frac{\text{MASS DRUG}}{A \cdot \text{TIME}} = -D \frac{\partial C}{\partial x}$$

$$J = \frac{dQ}{dt} \frac{1}{A}$$

Q = MASS OF DRUG A = SURF. AREA OF MEMBRANE

$$\frac{dQ}{dt} = \frac{AD}{\delta} (C_r - C_m)$$

↓ TOTAL AMOUNT RELEASED AT TIME t :

$$Q(t) = \frac{AD}{\delta} (C_r - C_m) t$$

$$\frac{dQ}{dt} = \text{CONSTANT! (ZERO-ORDER)}$$

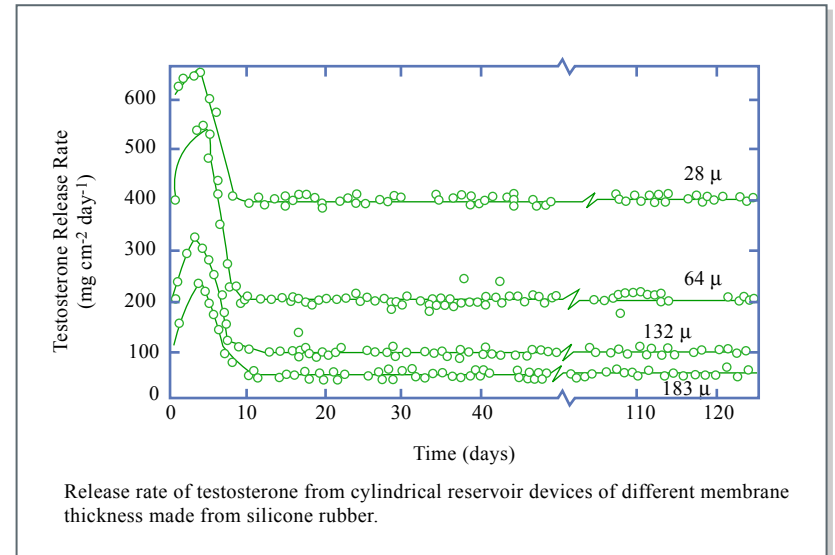
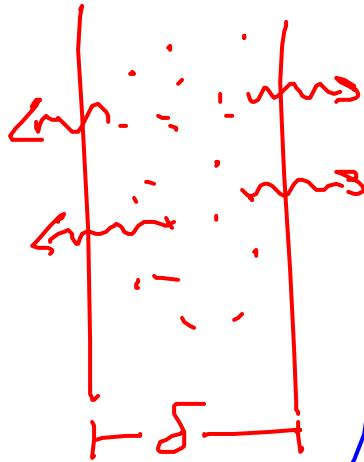


Figure by MIT OCW.

Release kinetics for diffusion-controlled release

MATRIX:



FICK'S 2ND LAW: $\frac{\partial c}{\partial t} = \nabla(D\nabla c)$

DRUG DISSOLVED IN MATRIX, NEGLECTING "END" EFFECTS:

$$Q = Q_{\infty} \left[1 - \sum_{n=0}^{\infty} \frac{8}{(2n+1)^2 \pi^2} \exp\left(-\frac{D(2n+1)^2 \pi^2 t}{\delta^2}\right) \right]$$

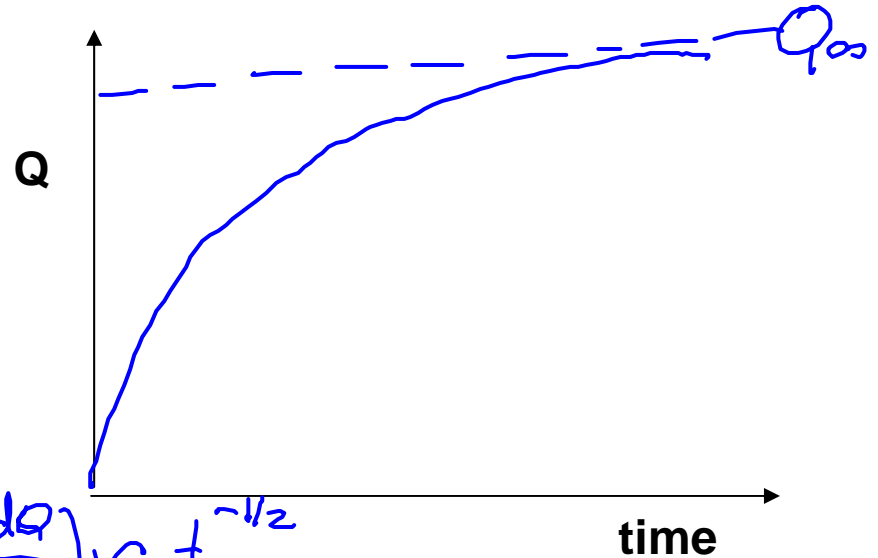
"SHORT TIMES"

$$\left(0 < \frac{Q}{Q_{\infty}} \leq 0.6\right)$$

↑
AMOUNT
RELEASED
AT $t = \infty$

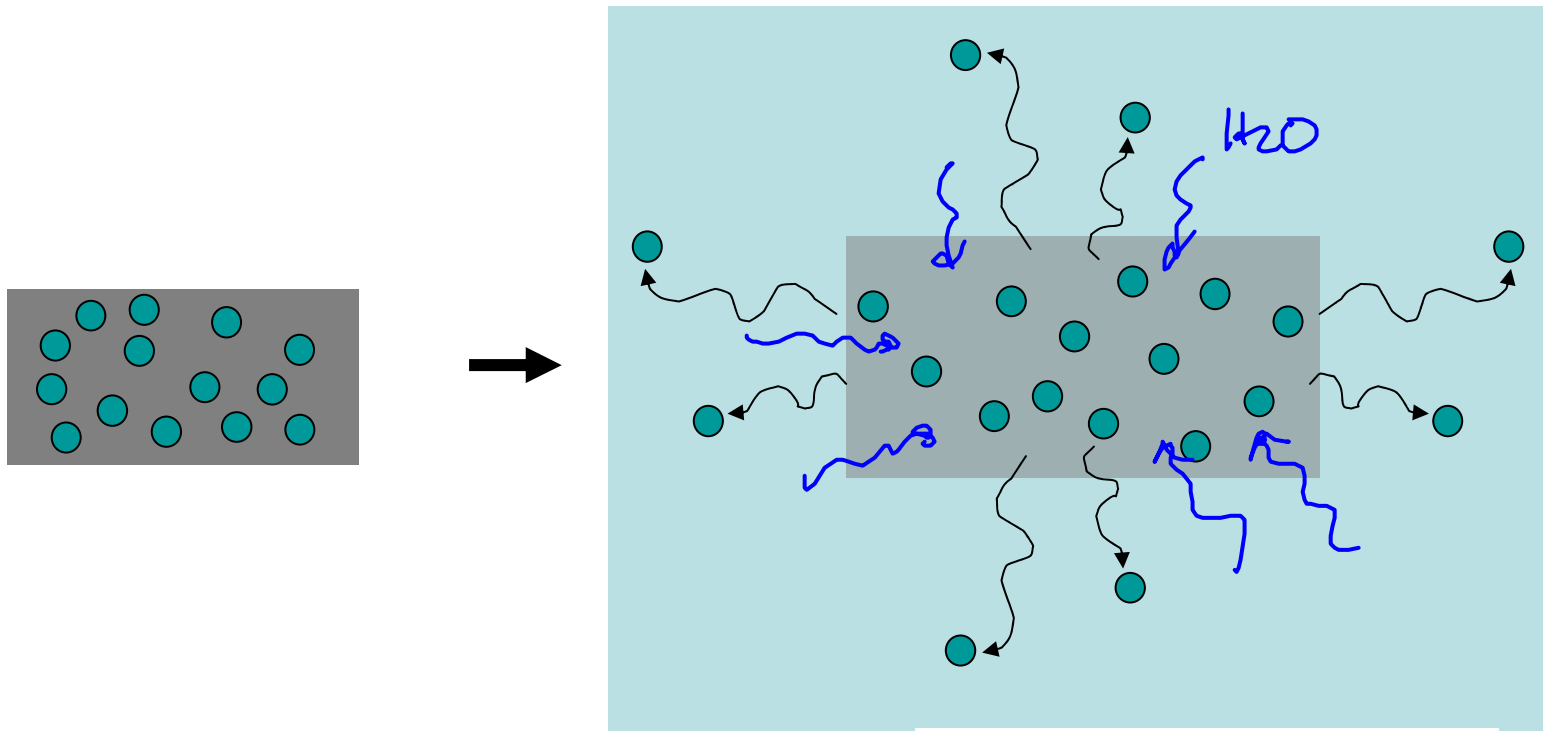
$$\frac{Q}{Q_{\infty}} \approx 4 \left(\frac{Dt}{\pi \delta^2} \right)^{1/2}$$

RATE: $\left(\frac{dQ}{dt}\right) \sim t^{-1/2}$

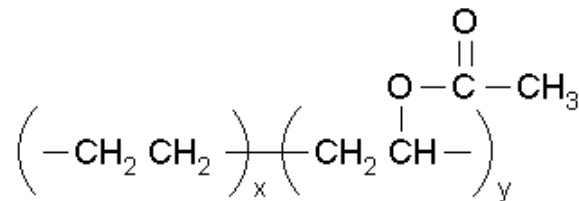


Water-influx controlled release

HYDROPHILIC MOLECULES RELEASED
BY H₂O SWELLS THE MATRIX



Example: poly(ethylene-co-vinyl acetate)

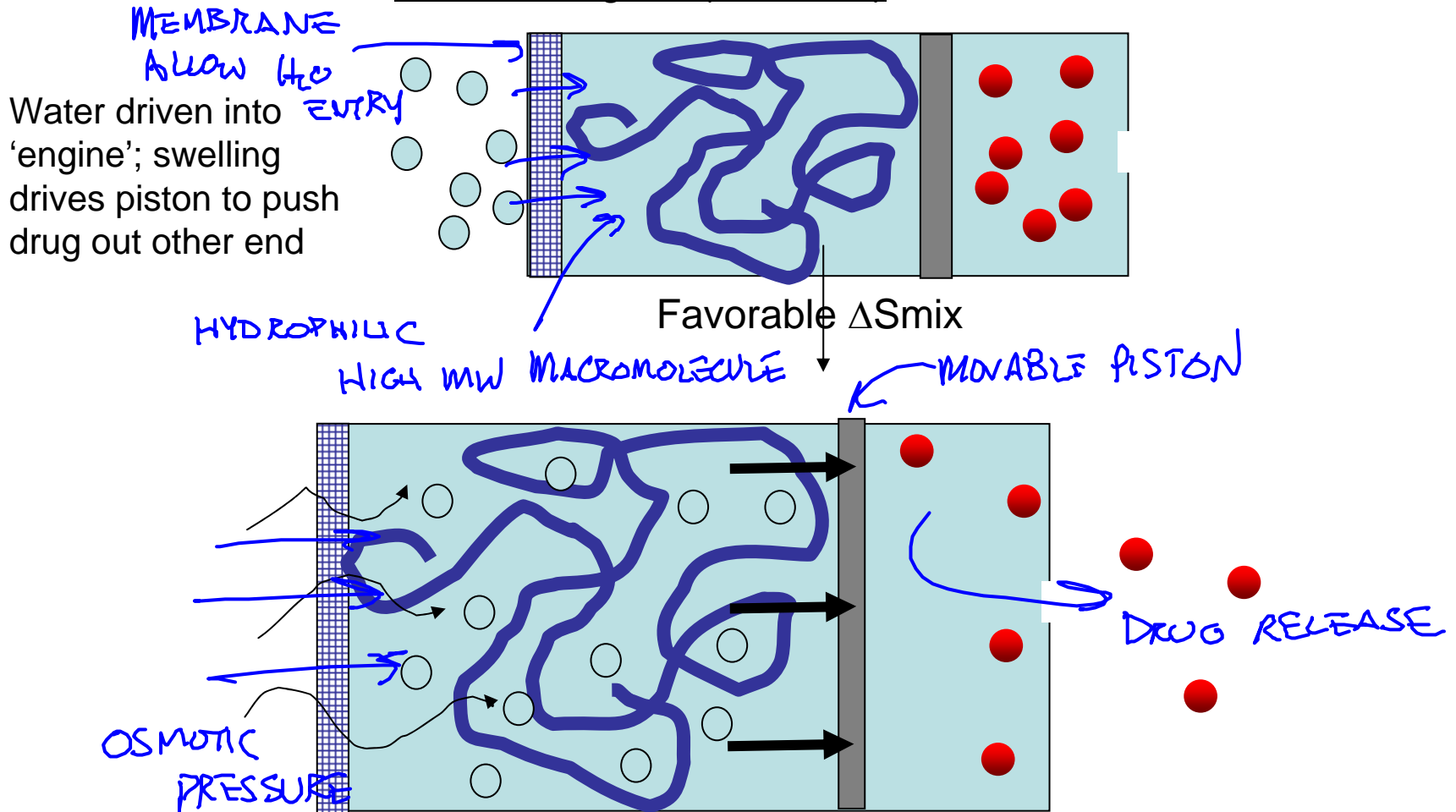


Regulated/triggered release: mechanical

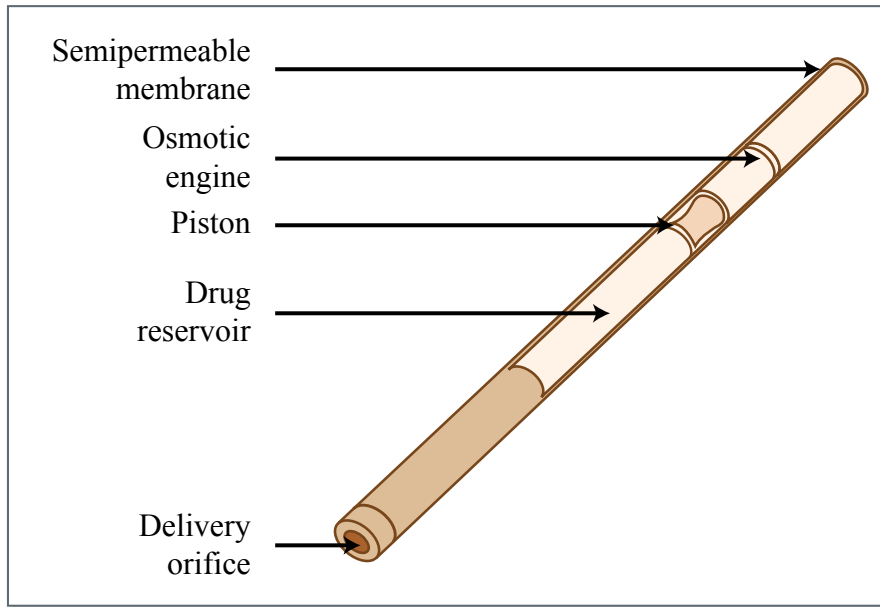
RELEASE HAPPENS IN RESPONSE TO A STIMULUS

- PROGRAMMED
- EXTERNAL

Osmotic engine: (one form)



Regulated/triggered release: mechanical



Designed to provide continuous release of drugs up to one year

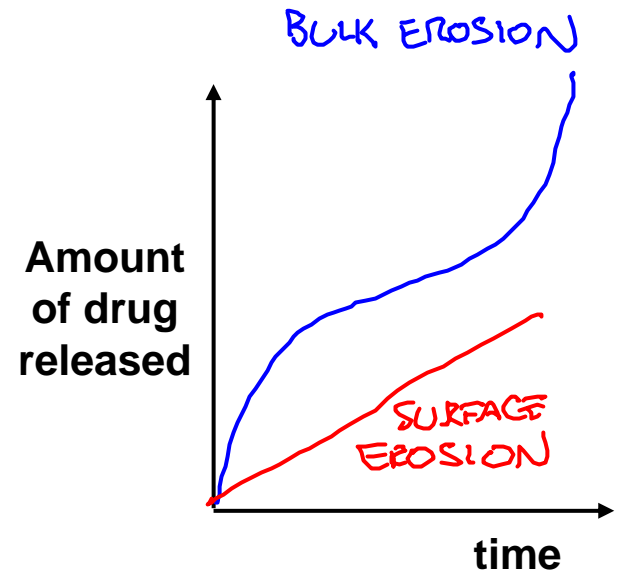
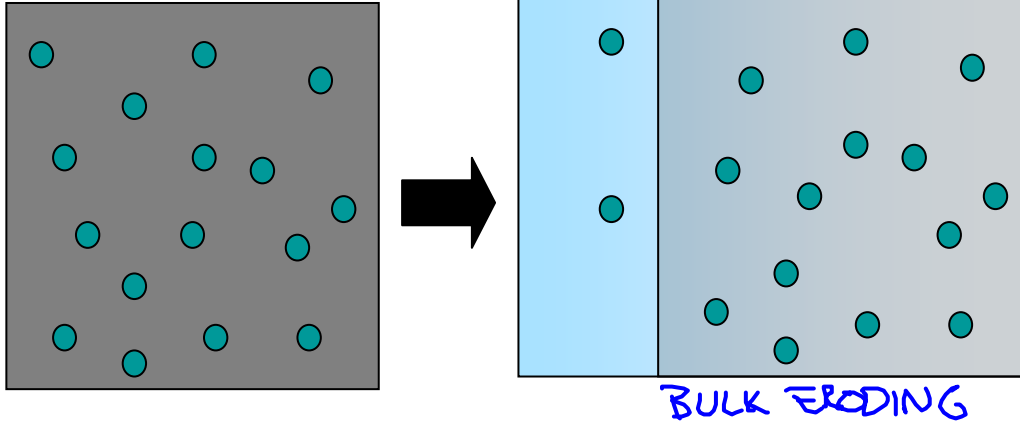
SEMI-ZERO ORDER
RELEASE
ACHIEVABLE

Figure by MIT OCW.

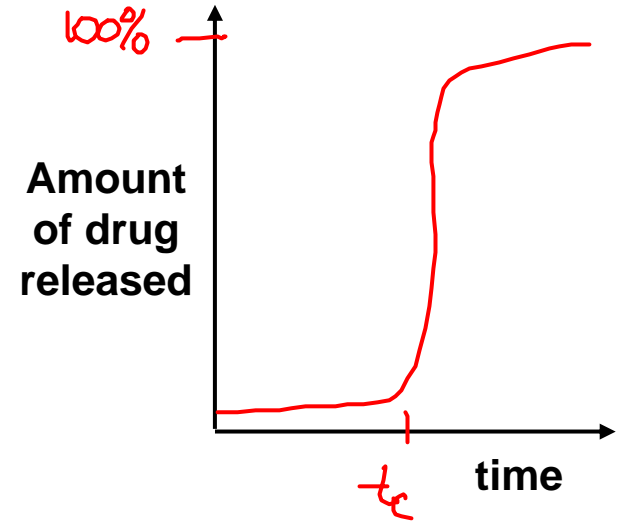
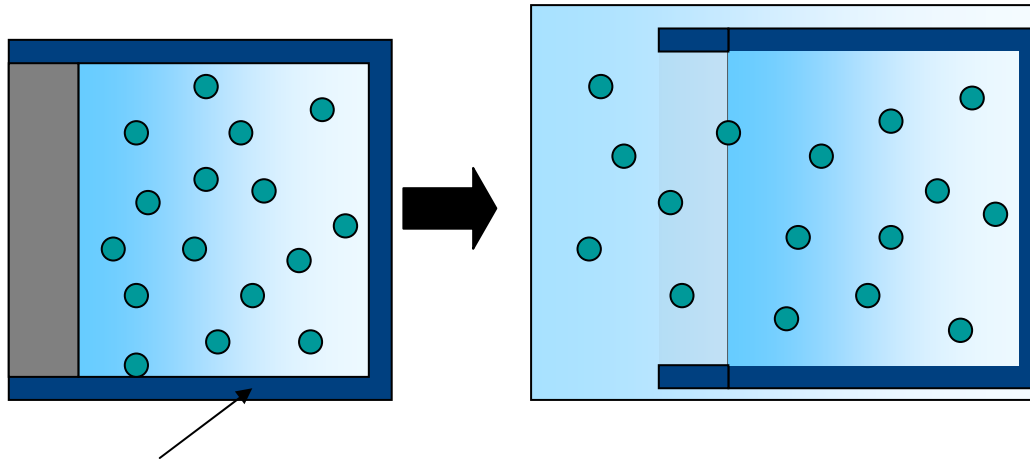
Titanium rod casing

eroding matrix

Continuous release:

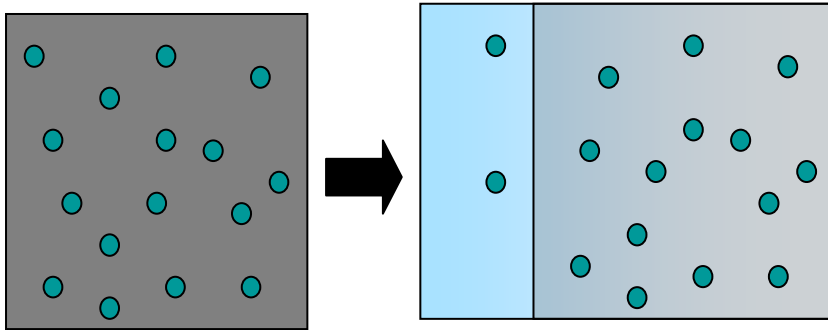


burst release:



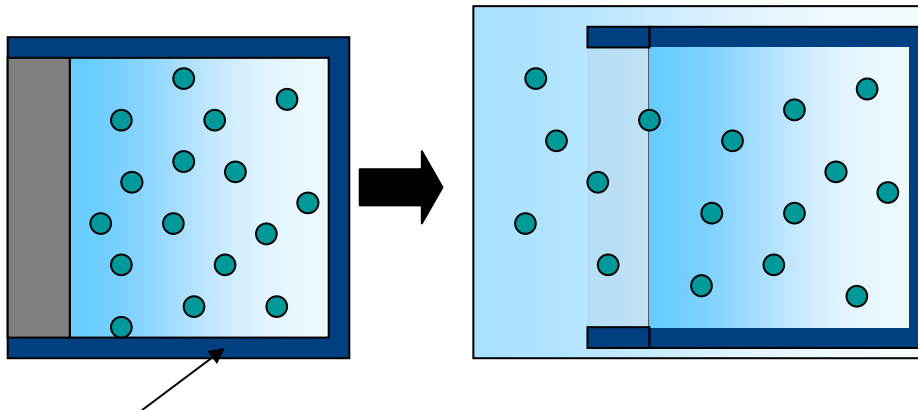
Non-erodible capsule

eroding matrix



Advantages:

- CAN BE INJECTABLE AND DEGRADABLE
- LOW DANGER OF DOSE DUMPING RELATIVE TO RESERVOIR DEVICE

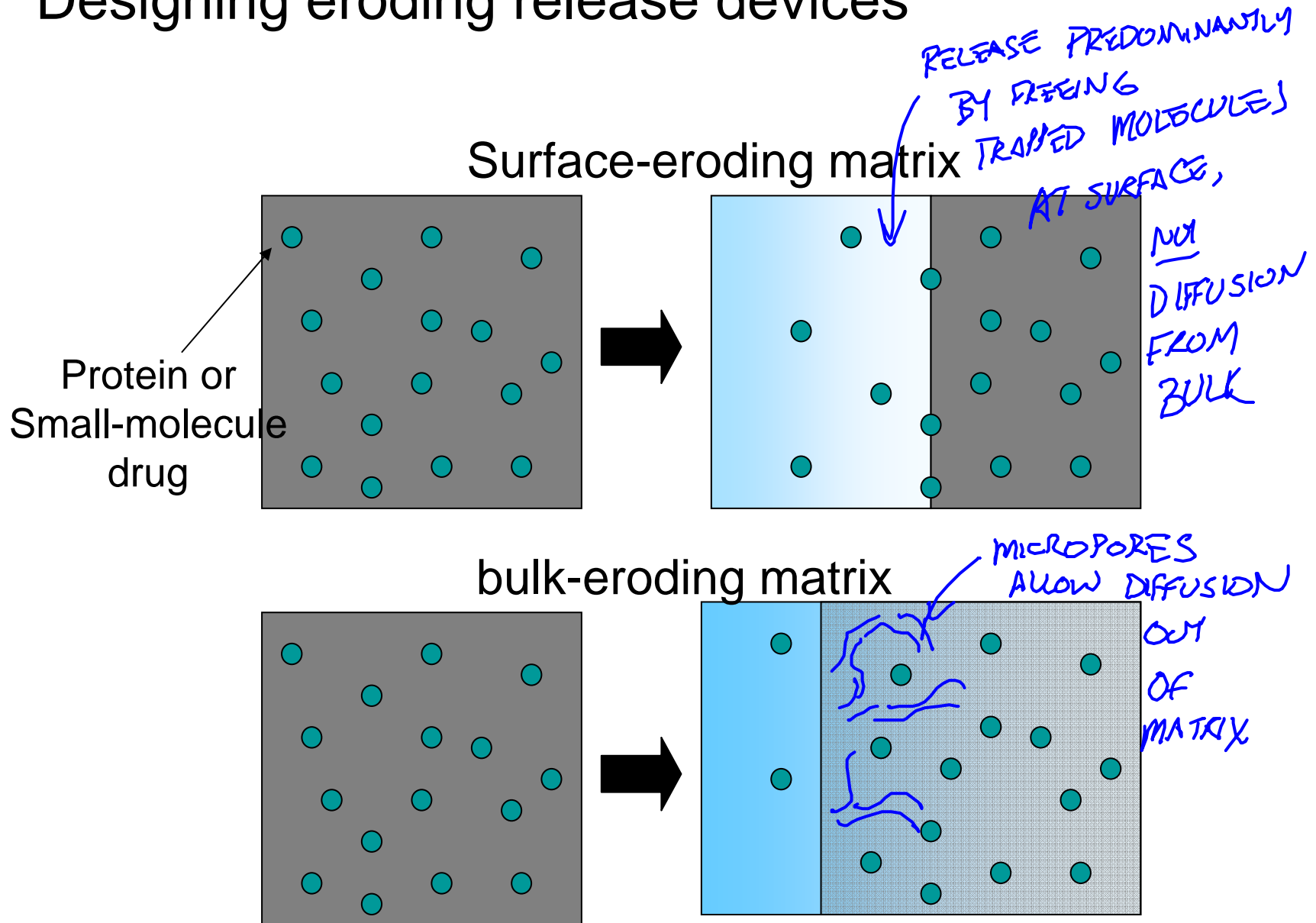


Disadvantages:

- OFTEN DIFFICULT TO STOP THERAPY UNTIL EROSION IS COMPLETE
- RELEASE WILL VARY W/ TIME, FOR BULK EROSION

Non-erodible capsule

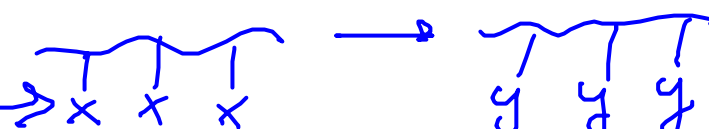
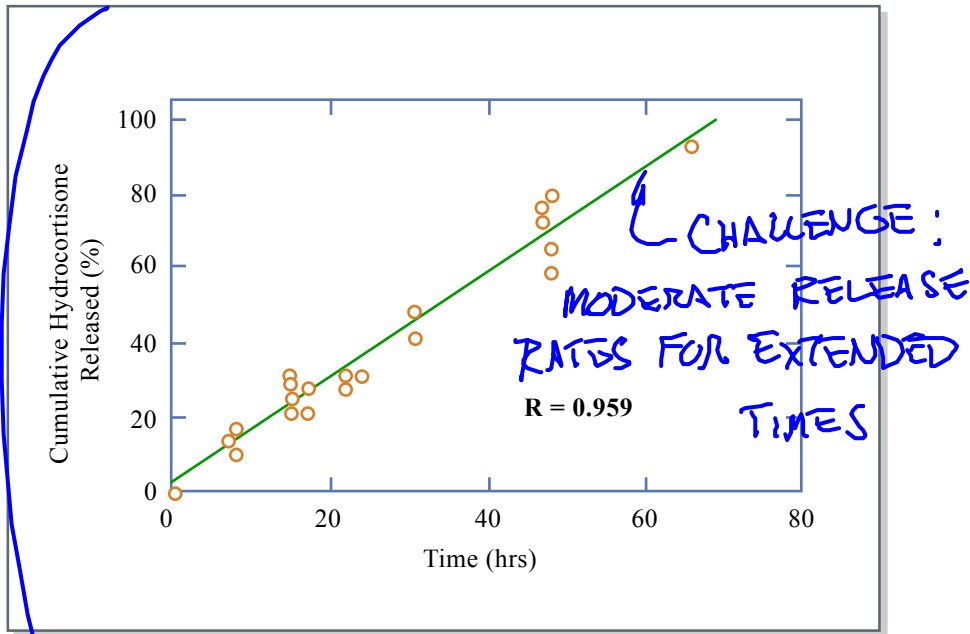
Designing eroding release devices



Typical release profiles

Surface-eroding matrix

Poly(methyl vinyl ether-co maleic anhydride)



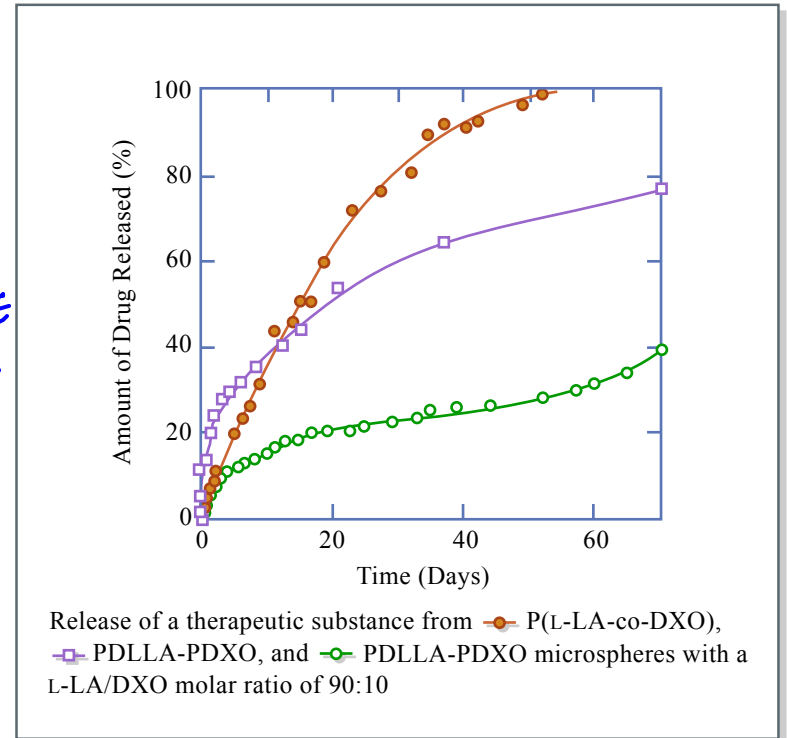
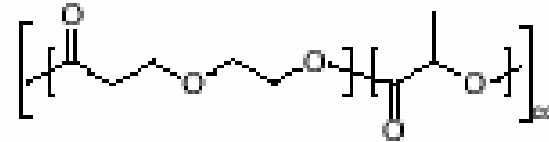
Garcia, J. T., M. J. Dorta, O. Munguia, M. Llabres, and J. B. Farina.

"Biodegradable Laminar Implants for Sustained Release of Recombinant Human Growth Hormone."

Biomaterials 23 (2002): 4759-4764.

Bulk-eroding matrix

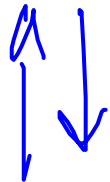
Poly(dioxepanone-co-lactide)



Characteristics of surface vs. bulk-eroding controlled release: (why not always use surface-eroding polymers?)

surface erosion:

~~0~~ -ORDER RELEASE



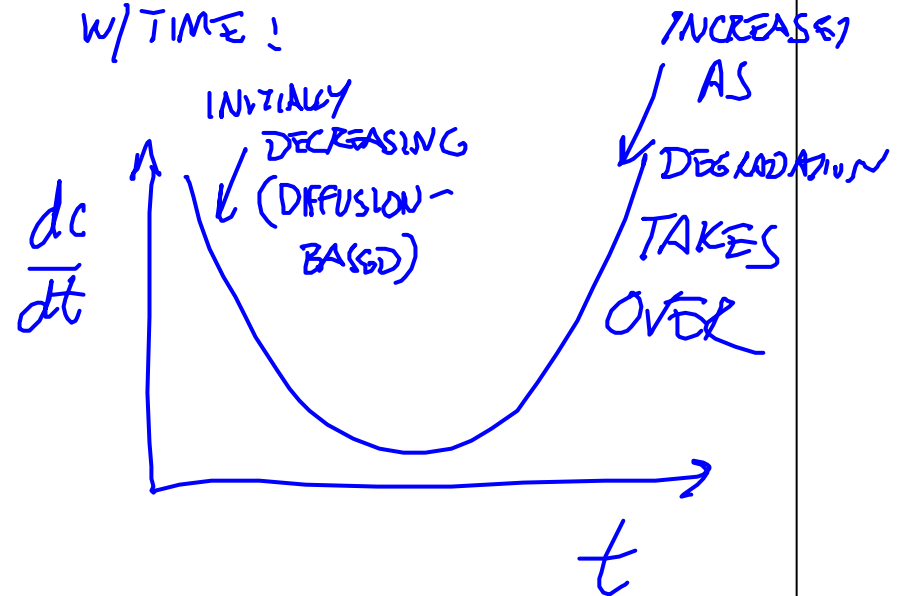
RAPID HYDROLYSIS

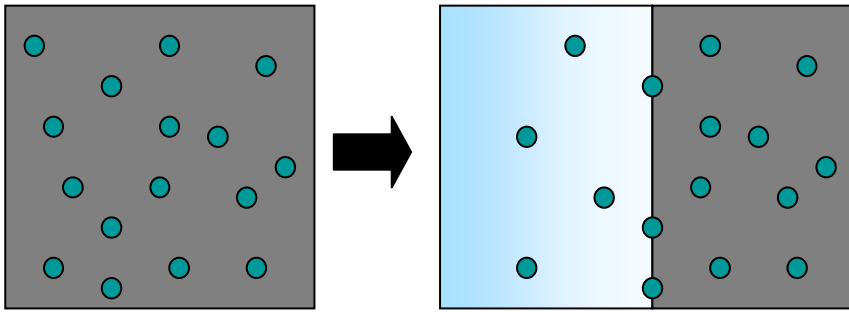
∴ SHORT LIFETIMES
FOR DELIVERY

bulk erosion

RELEASE RATE VARIES

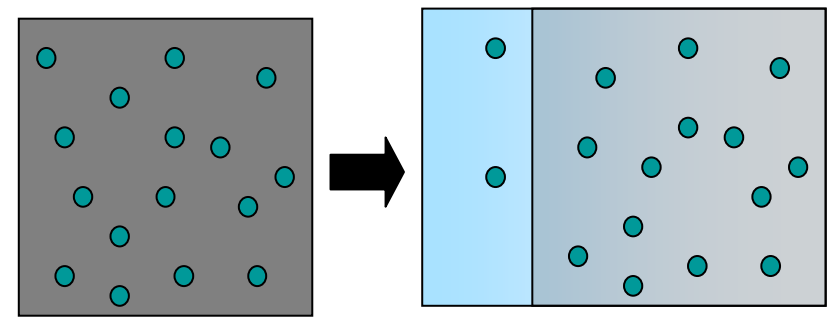
W/TIME!





Surface-eroding matrix

Poly(methyl vinyl ether-co maleic anhydride)



Bulk-eroding matrix

Poly(dioxepanone-co-lactide)

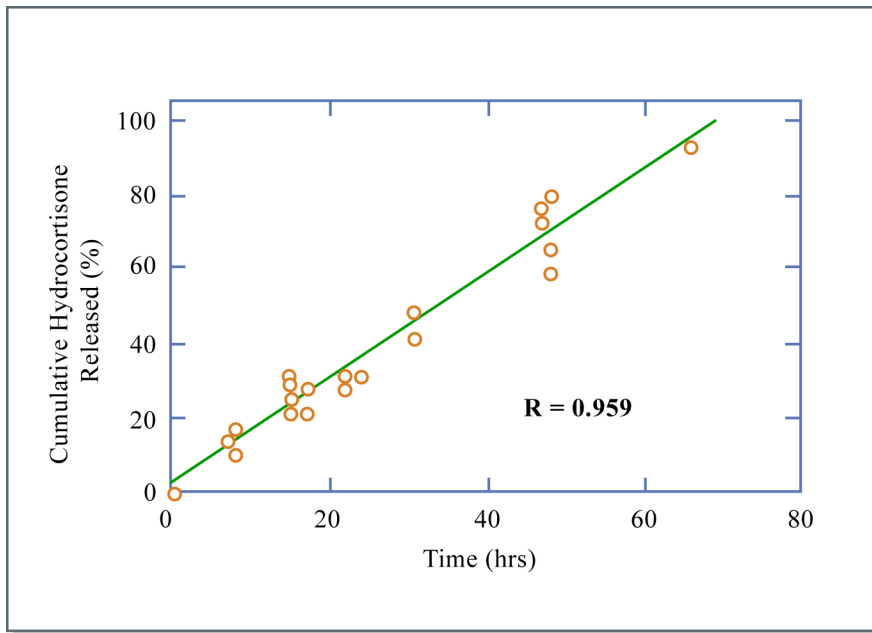
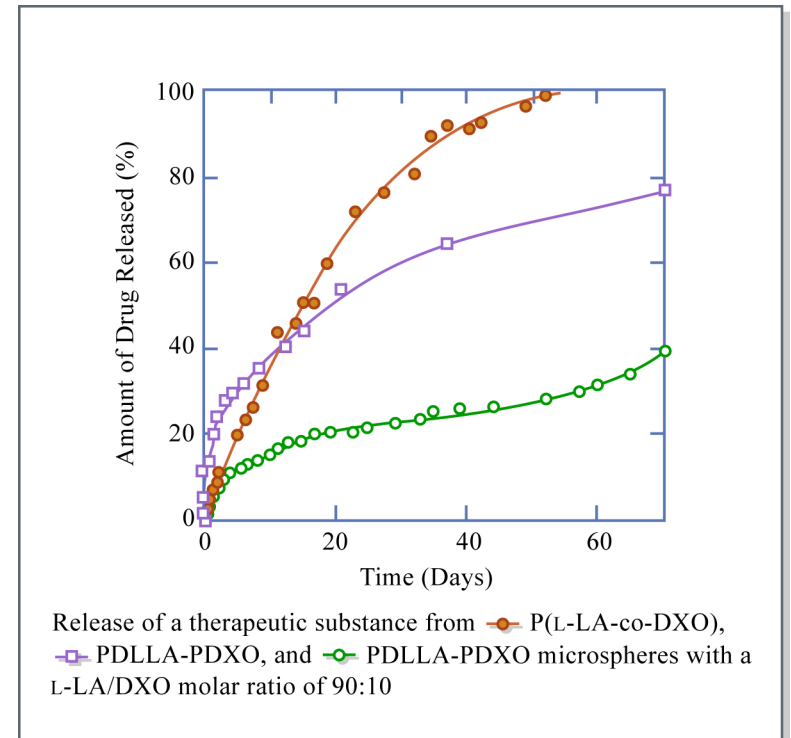
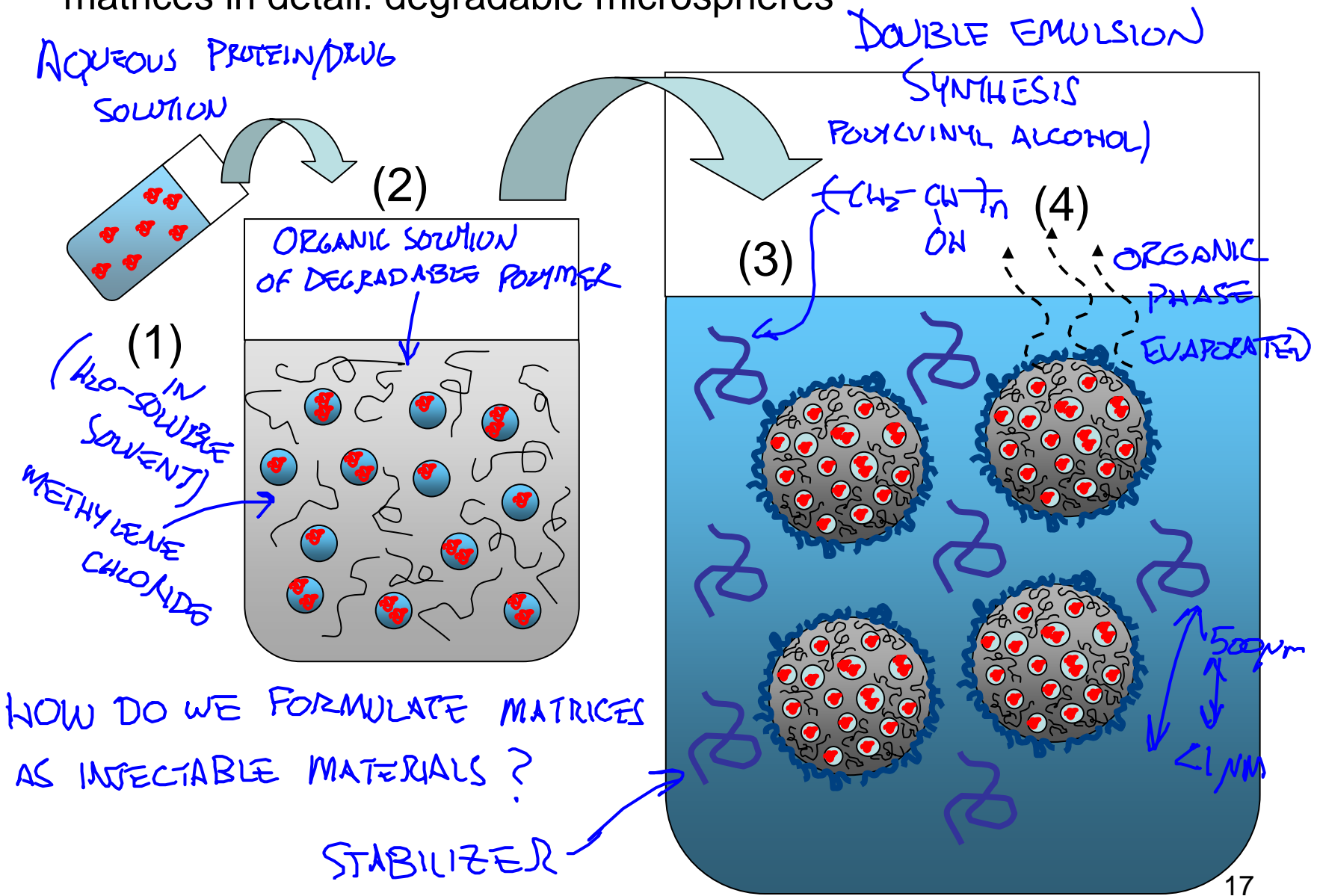


Figure by MIT OCW.



Release of a therapeutic substance from —●— P(L-LA-co-DXO), —□— PDLLA-PDXO, and —○— PDLLA-PDXO microspheres with a L-LA/DXO molar ratio of 90:10

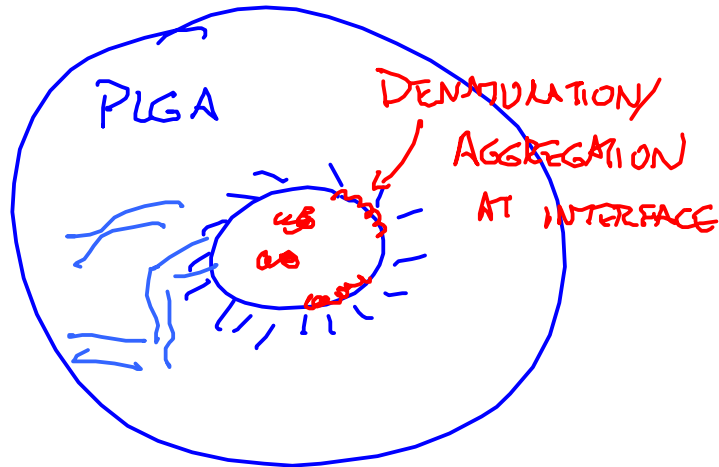
Examination of one approach to drug delivery using eroding matrices in detail: degradable microspheres



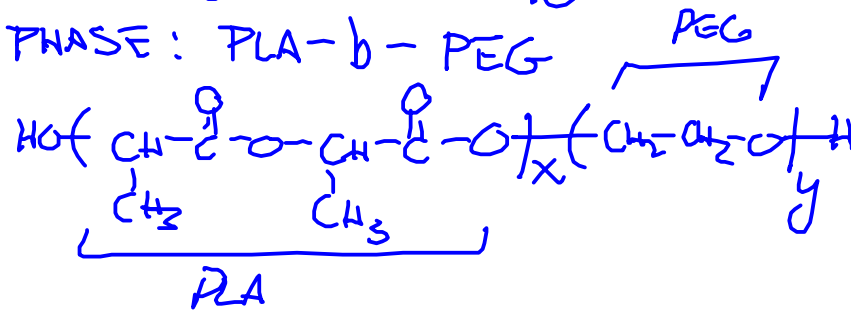
Limiting factors: pH gradients within degradable devices

Fu, K., D. W. Pack, A. M. Klibanov, and R. Langer. "Visual Evidence of Acidic Environment within Degrading Poly(lactic-co-glycolic acid) (PLGA) Microspheres." *Pharm Res.* 17, no. 1 (January 2000): 100-6.

Limiting factors: Contact with hydrophobic surfaces/organic interfaces



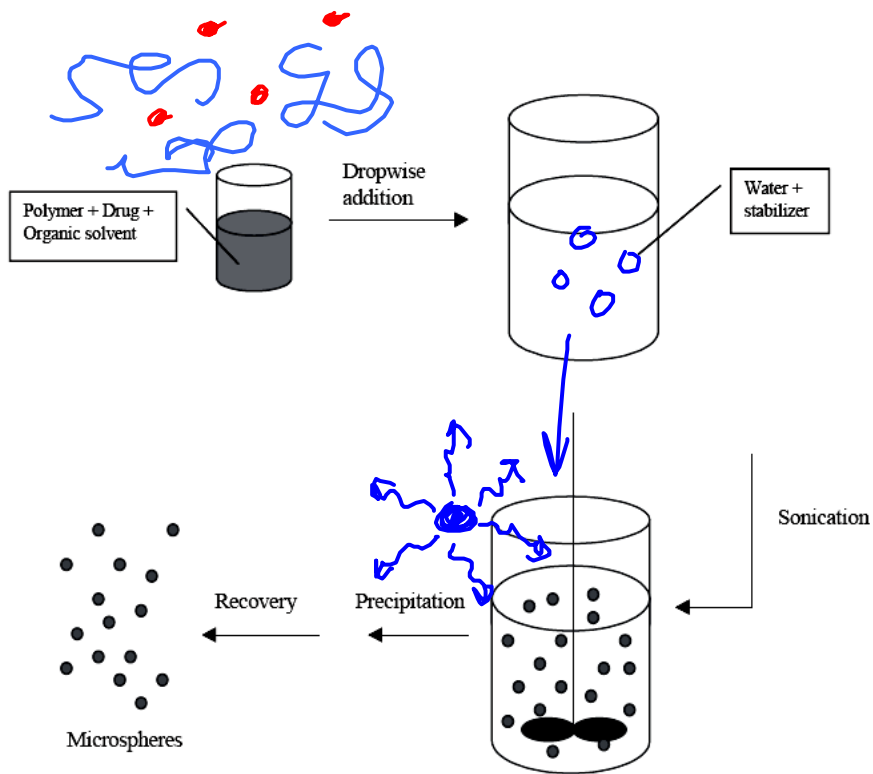
ADD AMPHIPHILIC BLOCK COPOLYMER TO ORGANIC PHASE: PLA-b-PEG



PEG FORMS STERIC BARRIER



Modeling an important controlled release system: single emulsion encapsulation of small molecule drugs in degradable polymers

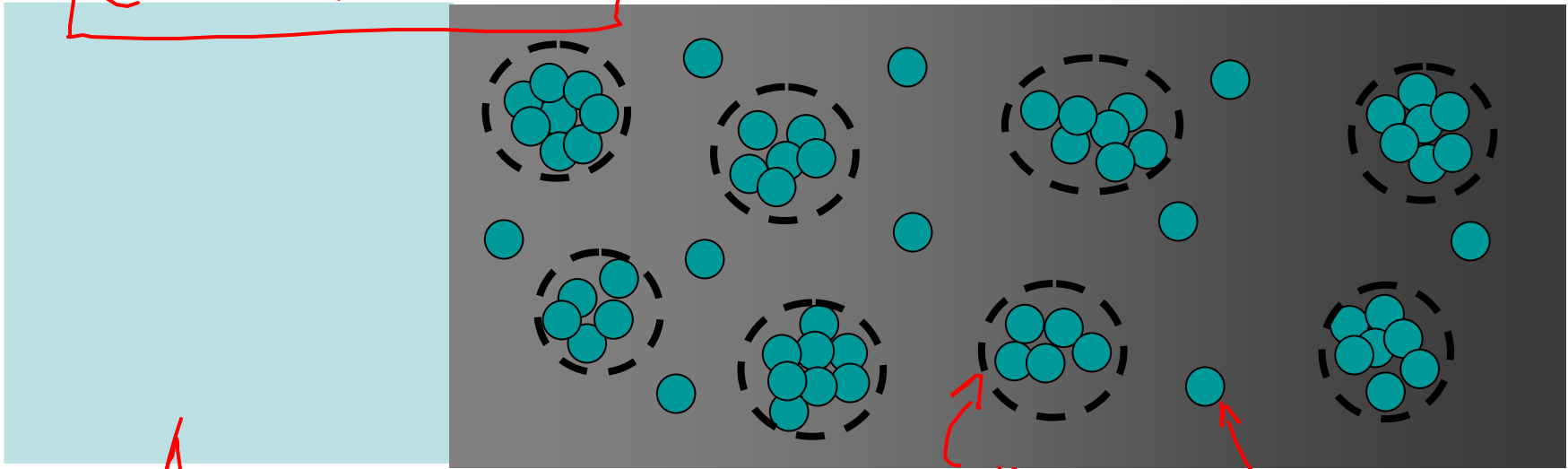


Faisant N., J. Siepmann, and J. P. Benoit. "PLGA-based Microparticles: Elucidation of Mechanisms and a New, Simple Mathematical Model Quantifying Drug Release." *Eur. J Pharm Sci.* 15, no.4 (May 2002): 355-66.

(Edlund 2002)

Theory of controlled release from degradable solids: physical basis of the model

CHARLIER MODEL → (EXTENSION OF HIGUCHI MODEL)



↑
INFINITE SINK
AT SURFACE

(WELL-MIXED VERY
LARGE RELEASE
MEDIUM)

DRUG
SOLID
PHASE

DRUG
DISSOLVED
IN MATRIX

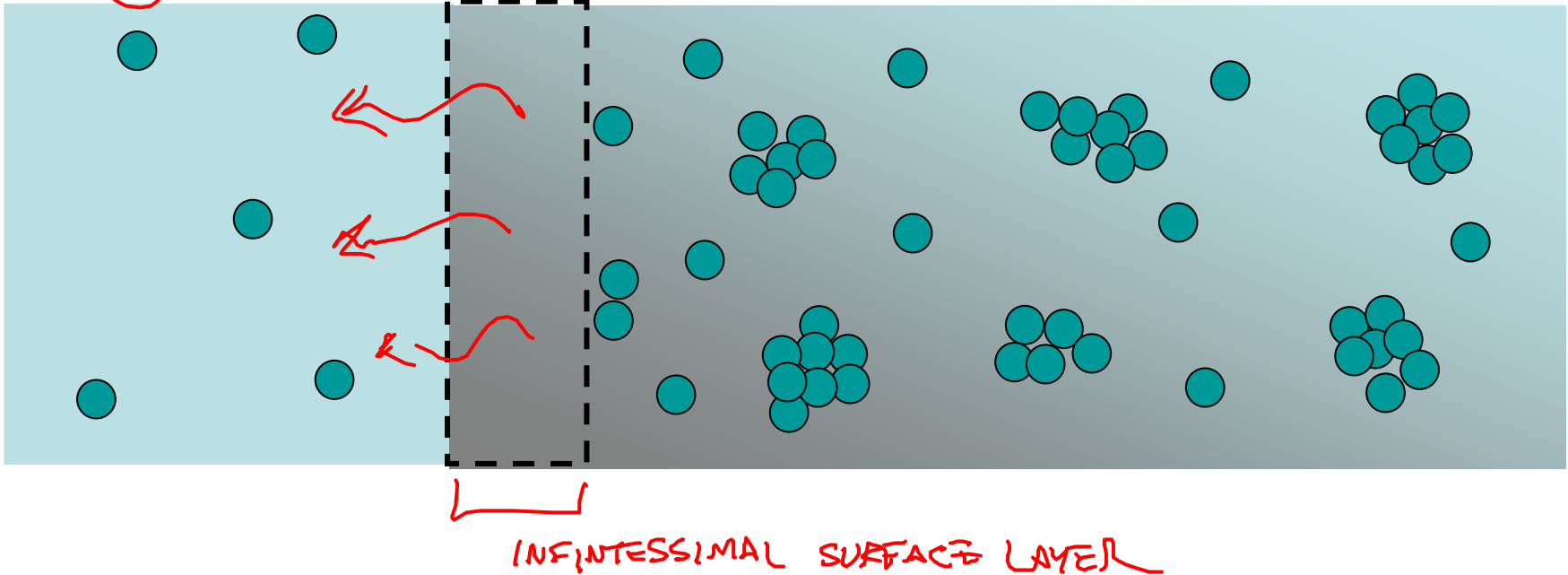
C_0 = OVERALL INITIAL DRUG CONC.
IN MATRIX

M_0 = INITIAL MW OF MATRIX

(Charlier et al. 2000)

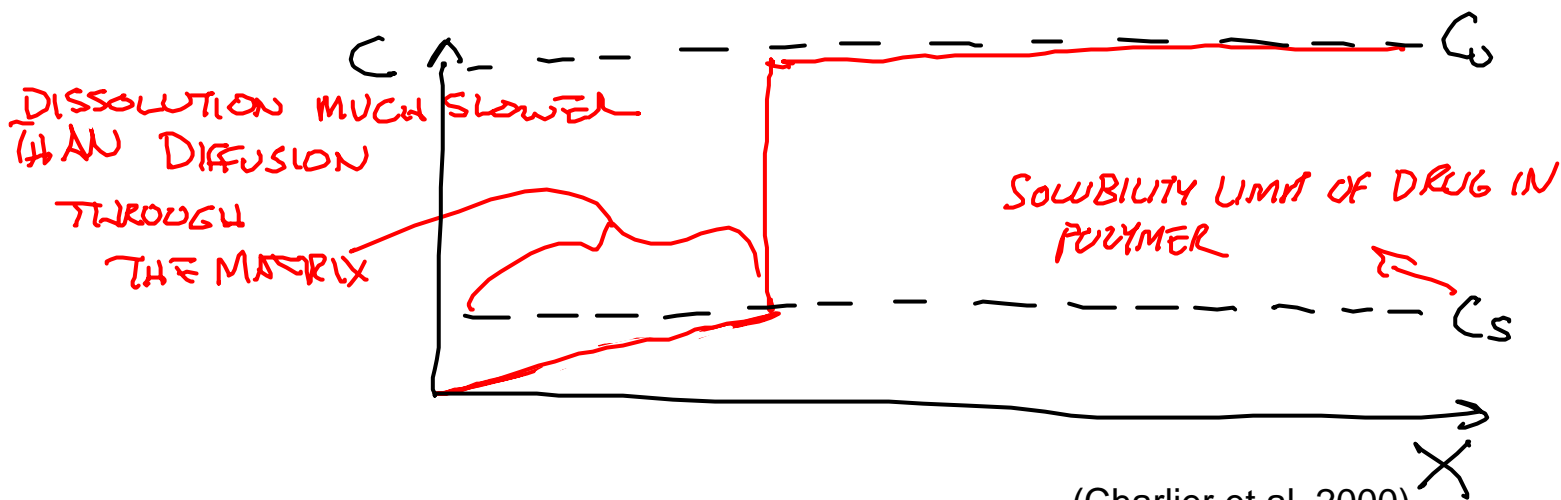
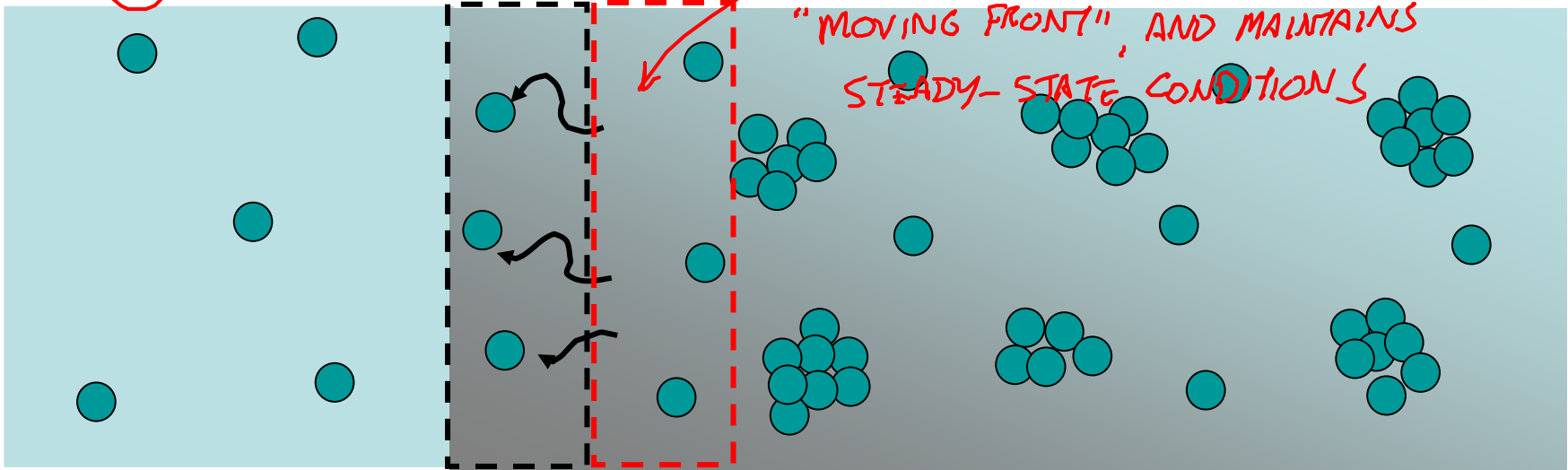
Theory of controlled release from degradable solids: physical basis of the model

① TIME ZERO: SURFACE LAYER EXTRACTION



Theory of controlled release from degradable solids: physical basis of the model

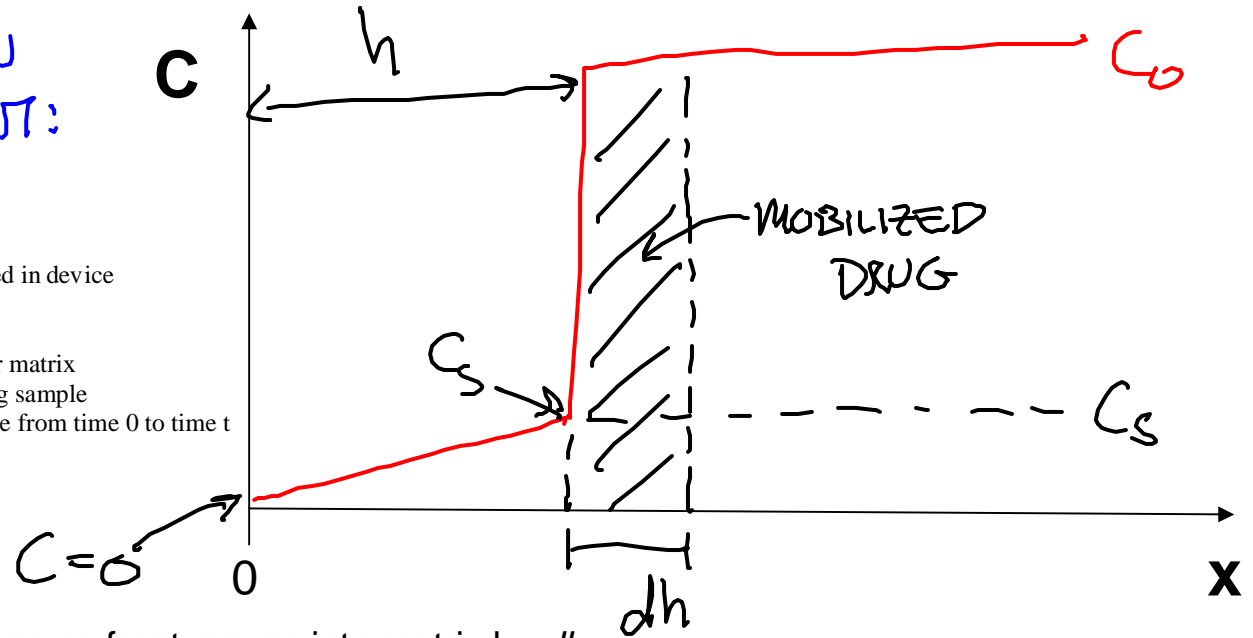
② DIFFUSION



MOTION OF DIFFUSION FRONT:

1. List of parameters:

- A device surface area
- C_s concentration of drug soluble in matrix
- C_0 initial concentration of drug encapsulated in device
- $M(t)$ molecular weight of matrix at time t
- M_0 initial molecular weight of matrix
- D Diffusion coefficient of drug in polymer matrix
- h thickness of diffusion region in releasing sample
- $Q(t)$ total mass of drug released from dispersed phase from time 0 to time t



Amount of drug freed to diffuse as front moves into matrix by dh :

$$\boxed{\text{I}} \quad dQ = C_0 A dh$$

Fick's first law in pseudo-steady-state diffusion region:

$$J = \frac{\text{MASS DRUG}}{A \cdot \text{TIME}} = \frac{1}{A} \frac{dQ}{dt} = -D \frac{dc}{dx} = -D \frac{(0 - C_s)}{h}$$

$$\frac{1}{A} \frac{dQ}{dt} = \frac{DC_s}{h} \quad \boxed{\text{II}} \quad \therefore dQ = \frac{A}{h} DC_s dt$$

Diffusion-controlled release for *nondegradable* solid: Higuchi equation

$$\boxed{\text{I}} \quad dQ = C_0 A dh$$

$$\boxed{\text{II}} \quad dQ = \frac{A}{h} D C_s dt$$

$$h \rightarrow h = h(t)$$

ASSUMING
NON-DEGRADABLE
MATRIX!

MASS BALANCE:

$$C_0 A dh = \frac{A}{h} D C_s dt$$

$$h' dh' = \frac{D C_s}{C_0} dt$$

$$\int_0^{h(t)} h' dh' = \int_0^t \frac{D C_s}{C_0} dt$$

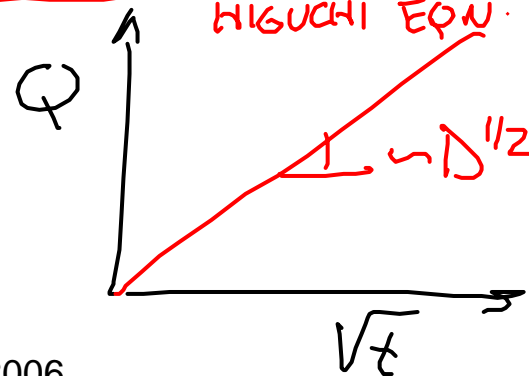
$$\boxed{\frac{h^2(t)}{2} = \frac{D C_s t}{C_0}}$$

PLUG INTO $\boxed{\text{II}}$:

$$dQ = \frac{A D C_s dt}{(2 D \frac{C_s}{C_0} t)^{1/2}}$$

$$Q(t) = 2^{1/2} A D^{1/2} C_s^{1/2} C_0^{1/2} t^{1/2}$$

HIGUCHI EQN.



Further Reading

1. Kumamoto, T. et al. Induction of tumor-specific protective immunity by in situ Langerhans cell vaccine. *Nat Biotechnol* **20**, 64-9 (2002).
2. Dash, P. R. & Seymour, L. W. in *Biomedical Polymers and Polymer Therapeutics* (eds. Chiellini, E., Sunamoto, J., Migliaresi, C., Ottenbrite, R. M. & Cohn, D.) 341-370 (Kluwer, New York, 2001).
3. Baldwin, S. P. & Saltzman, W. M. Materials for protein delivery in tissue engineering. *Adv Drug Deliv Rev* **33**, 71-86 (1998).
4. Okada, H. et al. Drug delivery using biodegradable microspheres. *J. Contr. Rel.* **121**, 121-129 (1994).
5. Santini Jr, J. T., Richards, A. C., Scheidt, R., Cima, M. J. & Langer, R. Microchips as Controlled Drug-Delivery Devices. *Angew Chem Int Ed Engl* **39**, 2396-2407 (2000).
6. Garcia, J. T., Dorta, M. J., Munguia, O., Llabres, M. & Farina, J. B. Biodegradable laminar implants for sustained release of recombinant human growth hormone. *Biomaterials* **23**, 4759-4764 (2002).
7. Jiang, G., Woo, B. H., Kang, F., Singh, J. & DeLuca, P. P. Assessment of protein release kinetics, stability and protein polymer interaction of lysozyme encapsulated poly(D,L-lactide-co-glycolide) microspheres. *J Control Release* **79**, 137-45 (2002).
8. Edlund, U. & Albertsson, A.-C. Degradable polymer microspheres for controlled drug delivery. *Advances in Polymer Science* **157**, 67-112 (2002).
9. Siepmann, J. & Gopferich, A. Mathematical modeling of bioerodible, polymeric drug delivery systems. *Adv Drug Deliv Rev* **48**, 229-47 (2001).
10. Charlier, A., Leclerc, B. & Couarraze, G. Release of mifepristone from biodegradable matrices: experimental and theoretical evaluations. *Int J Pharm* **200**, 115-20 (2000).
11. Fan, L. T. & Singh, S. K. *Controlled Release: A Quantitative Treatment* (eds. Cantow, H.-J. et al.) (Springer-Verlag, New York, 1989).